BRAIN-DERIVED MICROPARTICLES INDUCE SYSTEMIC COAGULATION IN A MURINE MODEL OF TRAUMATIC BRAIN INJURY

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KEY POINTS


2. Platelets facilitate the transmigration of brain microparticles through the endothelial barrier into the circulation.
**ABSTRACT:** Traumatic brain injury (TBI) is associated with coagulopathy, although it often lacks two key risk factors: severe bleeding and significant fluid resuscitation associated with hemorrhagic shock. The pathogenesis of TBI-associated coagulopathy remains poorly understood. We tested the hypothesis that brain-derived microparticles (BDMPs) released from an injured brain induce a hypercoagulable state that rapidly turns into consumptive coagulopathy. Here, we report that mice subjected to fluid percussion injury (1.9±0.1 atm) developed a BDMP-dependent hypercoagulable state, with peak levels of plasma glial cell and neuronal BDMPs reaching 17,496 ± 4,833/μl and 18,388 ± 3,657/μl, respectively, 3 hrs post TBI. Uninjured mice injected with BDMPs developed a dose-dependent hyper-turned hypo-coagulable state measured by a progressively prolonged clotting time, fibrinogen depletion, and microvascular fibrin deposition in multiple organs. The BDMPs were measured 50 – 300 nm with intact membranes, expressing neuronal or glial cell markers and procoagulant phosphatidylserine and tissue factor. Their procoagulant activity was greater than platelet microparticles and was dose-dependently blocked by lactadherin. Microparticles were produced from injured hippocampal cells, transmigrated through the disrupted endothelial barrier in a platelet-dependent manner, and activated platelets. These data define a novel mechanism of TBI-associated coagulopathy in mice, identify early predictive markers and provide alternative therapeutic targets.
INTRODUCTION

Uncontrolled hemorrhage is a leading cause of the preventable deaths that occur in patients with trauma, accounting for 30-40% of all trauma fatalities.\textsuperscript{1,2} It is caused by direct injury to the vasculature and a resulting secondary coagulopathy. The causes of trauma-associated coagulopathy include blood loss, consumption of coagulation factors and platelets, the dilution of coagulation factors and platelets due to fluid resuscitation, and hypothermia.\textsuperscript{3,4} Recent studies also implicate a role of activated protein C in the coagulopathy associated with severe trauma.\textsuperscript{5,6}

Retrospective and observational studies have consistently shown that coagulopathy is common in patients with traumatic brain injury (TBI).\textsuperscript{7-11} However, isolated TBI lacks two key causal factors for coagulopathy associated with injury to the trunk and limbs: heavy blood loss and a large volume of fluid resuscitation, suggesting that it follows a distinct pathogenic pathway. The finding that coagulopathy is common in patients with penetrating brain injury\textsuperscript{10} further indicates that damage to cerebral tissue plays a role in developing the coagulopathy. In a study of 972 TBI patients with coagulopathy, D-dimer and fibrinogen degradation products were detected minutes after injury, followed by a profound depletion of fibrinogen.\textsuperscript{8} Prolonged prothrombin and partial thromboplastin times usually occurred late, indicating a transition from a hyper- to a hypo-coagulable state.\textsuperscript{8,9}

Despite strong clinical and laboratory evidence of its presence and association with poor clinical outcomes,\textsuperscript{12} the pathogenesis of TBI-associated coagulopathy remains
poorly understood. Current clinical tests detect the coagulopathy, but are insufficient to
determine its causes or to predict its occurrence, making clinical management of TBI-
associated coagulopathy difficult and costly. We hypothesized that brain-derived
procoagulant molecules delivered in the form of cellular microparticles play a role in
developing systemic coagulopathy after TBI. This hypothesis is derived from several
observations. First, the brain is enriched in procoagulant anionic phospholipids, such as
phosphatidylserine (PS), which provide a negatively charged surface to initiate and
propagate coagulation.13 These anionic phospholipids are normally present on the inner
leaflet,14 whereas neutral phospholipids, such as phosphatidylcholine (PC) and
sphingomyelin, are on the external leaflet of the cell membrane.15 This asymmetry is
lost in cells subjected to traumatic and/or ischemic injuries, exposing PS on the outer
membrane.16 Second, tissue factor (TF), which initiates the extrinsic pathway of
coagulation on platelets, is also richly expressed on neurons and glial cells.17-19 A long-
standing question is how TF and PS are integrated into the membrane of activated
platelets, which express no or an extremely low level of TF,20;21 in order to initiate the
coagulation during trauma hemostasis. One potential mediator is cellular microparticles.

Microparticles are cell fragments produced from activated or apoptotic cells.22;23 They
are primarily composed of the plasma membrane along with a limited amount of
cytoplasm and measure 0.1 to 1 μm in diameter.23 They are enriched in the lipid micro-
domains, where cholesterol, phospholipids, and receptors are clustered.24;25 These
microparticles promote coagulation by providing PS-dependent binding sites for the
assembly of a prothrombinase and tenase complex26 and by adhering to or fusing with
the platelet membrane. While microparticles from blood cells have been detected at high levels in TBI patients, those released from an injured brain have not been studied. Neural cells are highly sensitive to mechanical and ischemic injuries, potentially leading to microvesiculation. However, it is not known whether 1) an injury induces neural cells to vesiculate, 2) brain-derived microparticles (BDMPs) are released into the systemic circulation, and 3) BDMPs induce intravascular coagulation. Here, we report that highly procoagulant BDMPs are detected in the systemic circulation and induce coagulation in mice either subjected to TBI or infused with BDMPs.
MATERIALS AND METHODS

A mouse model of FPI

Adult male C57BL/6J mice (12-16 wks and 22-25g, Jackson Laboratory, Bar Harbor, ME) were subjected to fluid percussion injury (FPI)\(^3\). Briefly, a mouse was anesthetized by ketamine and xylazine (1 mg and 0.1 mg/10g) on a ventilator (Harvard Apparatus, Hollistone, MA) and constrained to a platform to surgically expose the skull. A 3-mm diameter hole was drilled into the skull (2.0-mm posterior from the bregma and 2.0-mm lateral to the sagittal suture) with the dura matter intact. A female Leur-Lok was cemented to the craniotomy site of the mouse that had been allowed to recover from the surgery for 60 min and was connected to an FPI device (Custom Design & Fabrication, Richmond, VA). With the head unrestrained, saline from a Plexiglas cylindrical reservoir was rapidly injected into the closed cranial cavity at a controlled pressure of 1.9 ± 0.1 atm. A sham mouse underwent the same surgery without being exposed to FPI. To model the acute events and to minimize impacts of secondary injury, all mice were examined within the first 6 hrs after FPI. The mouse study is approved by the IACUC of PSBC.

Detection of brain-derived microparticles

Neuron- and glial cell-derived microparticles (collectively termed BDMP) were identified by a modified flow cytometry-based method (Fig. S1).\(^3\) They were first identified by their size (< 1 μm) using standard microbeads that were 0.5, 0.9, and 3 μm in diameter (Biocytex, Marseille, France) and then by their expression of neuron specific enolase (NSE) and glial fibrillary acidic protein (GFAP) using FITC-conjugated monoclonal
(Abcam, Cambridge, MA) and polyclonal antibodies (eBioscience Inc., San Diego, CA) on an LSR II flow cytometer (Beckon Dickinson, San Jose, CA, Fig. S8). Isotype specific IgGs and a rabbit non-immune IgG were used as negative controls. To reduce small particle contaminants, buffers were filtered with a 0.1 \( \mu \text{m} \) filter (EDM Millipore, Billerica, MA) before use. The data were presented as the percent of Annexin V+ and neural marker+ microparticles in the microparticle gate set by microbeads unless otherwise specified. To validate the data and address the concern that NSE is also expressed in platelets and erythrocytes\textsuperscript{35,36}, BDMPs were also probed with monoclonal antibodies against the neuronal marker Na\textsuperscript{+}/K\textsuperscript{+} ATPase \( \alpha 3 \), and the glial marker glutamate transporter 1 (both from EMD Millipore).

The expression of TF and PS on BDMPs were detected using a PE-conjugated polyclonal antibody (Bioss, Inc., Woburn, MA) and APC-conjugated Annexin V (eBioscience), respectively. EDTA (5 mM) was used to test the specificity of this assay (Fig. S2). BDMPs were quantified by double-labeling with antibodies to GFAP/NSE and annexin V binding.

**Coagulation assays**

Two coagulation assays were performed to evaluate BDMP-associated procoagulant activity in order to assess relative contributions of PS and TF. The first was a PS-dependent assay that tested the ability of BDMPs to promote clot formation in the presence of coagulation factor Xa.\textsuperscript{37} For each reaction, 25 \( \mu \text{l} \) of phosphate-buffered saline (PBS) containing a known number of BDMPs were mixed with 25 \( \mu \text{l} \) of
phospholipid-deficient porcine plasma (IMVS, Adelaide, Australia) and 100 μl of bovine factor Xa (0.02 U/ml in a buffer containing 15 mM CaCl₂, 100 mM NaCl, 20 mM HEPES, and 0.001% polybrene [pH 7.0]). Clot formation was monitored at 37°C on a CoaScreener coagulation analyzer (American Labor Corp., Durham, NC). Purified brain PS and PC (Avanti Polar Lipids, Inc. Alabaster, AL) were used as positive and negative controls, respectively. The calcium dependence of this assay was determined by treating samples with 4 mM of EDTA (Fig. S3). For mouse experiments, blood collected after injury or infused with BDMPs was centrifuged at 1,500 x g for 20 min at 25°C to collect platelet-poor plasma (PPP). PPP was either tested directly or processed to generate microparticle-free plasma (MPFP). To obtain MPFP, PPP was centrifuged at 13,000 x g for 2 min at room temperature to obtain the cell-free supernatant, which was centrifuged twice at 100,000 x g (4°C, 60 min) to remove microparticles. The second assay measured the ability of BDMP-bound TF to promote thrombin generation in the presence of phospholipids using a commercial kit (Supplemental method).³⁸

**Binding of lactadherin to BDMPs**

FITC-conjugated bovine lactadherin (Haematologic Technologies, Inc., Essex Junction, Vermont) was incubated with purified BDMPs for 30 min and then with a PE-conjugated monoclonal glutamate transporter 1 antibody (EMD Millipore) for 20 min. Lactadherin binding was detected by FITC fluorescence on glutamate transporter 1⁺ BDMPs in the absence and presence of a ~100-fold excess unlabeled lactadherin (Haematologic Technologies) or increasing concentrations of brain PS and PC.
Culture of neural cells and microparticle production

Hippocampi were dissected from euthanized newborn C57BL/6J mice and washed with PBS. They were incubated for 20 min at 37°C with Hibernate A medium containing 2% B27 serum-free supplement (Life Technologies, Grand Island, NY), 0.5 mM L-glutamine (Life Technologies) and 2 mg/ml papain (Worthington Biochemical Corp., Lakewood, NJ). Partially digested-hippocampi were incubated with 0.2 mg/ml DNAse I for 5 min at 37°C and dispersed into a homogenous cell suspension. After viability measured using a trypan blue exclusion test, 2 – 4 x 10^5 viable cells were plated on a 35-mm culture dish coated with 50 μg/ml of poly-D-lysine (Sigma Aldrich, St. Louis, MO) and cultured in Neurobasal-A medium (2% B27 serum-free supplement, 0.5 mM L-glutamine and 5 ng/ml basic fibroblast growth factor, Life Technologies) at 37°C. After 7 days in culture, cells were washed with PBS and stimulated with 15 μM of the calcium ionophore A23187 (Fisher Bioreagents, Waltham, MA), which served as a surrogate for cell injury, for 30 min at 37°C. Media from the stimulated and unstimulated cells were collected and centrifuged at 16,000 x g for 10 min. Microparticles in the supernatant were detected by flow cytometry.

BDMP transmigration through the endothelial cell barrier

PKH26 (Sigma-Aldrich Corp., St. Louis, MO) has a long aliphatic tail that stably incorporates into lipid regions of the cell membrane, emitting yellow-orange fluorescence. BDMPs were incubated with 5 μM PKH26 for 5 min at room temperature. The labeling was stopped by the addition of 500 μl of 10% BSA (1 min at room
temperature). PKH26-labeled BDMPs were collected by centrifugation at 100,000 x g for 1 h at 4°C and re-suspended in PBS for immediate experiments.

For transmigration experiments, HUVECs (Lonza, Basel, Switzerland) were grown in EBM-2 medium (Lonza) on a collagen-coated PTFE membrane (0.4 µm pore) that forms the base of a transwell (Corning, Tewksbury, MA). Confluent HUVECs were stimulated with 25 µM of histamine for 20 min at 37°C. After washing, PKH26-labeled BDMPs at 1 x 10⁷/ml were incubated with resting and activated HUVECs in the presence and absence of live or lyophilized platelets (300,000/µl) for 3 hrs at 37°C. The medium in the bottom chamber was collected and analyzed for BDMPs by flow cytometry (Fig. S4).

**Effects of BDMPs on platelets**

Human blood samples were collected in 0.38% sodium citrate from healthy subjects under an approved IRB protocol. They were centrifuged at 150 x g for 15 min at 25°C to collect PRP. Platelet counts were normalized to 2.5 x 10⁶/µl using homologous plasma.

Platelet aggregation induced by 1 x 10⁴/µl of BDMPs, in the presence and absence of type I collagen (Helena Laboratories, Beaumont, TX) was monitored at 37°C for 10 min in an AggRAM optical aggregometer (Helena Laboratories). To measure CD62p and PS expression, platelets were incubated with 1 x 10⁴/µl BDMPs in the presence of either a PE-conjugated CD62p antibody (BD Biosciences, San Jose, CA) or APC labeled-annexin V for 30 min at 37°C. The calcium influx in platelets induced by BDMPs was measured using a commercial probe (supplemental method).
To measure BDMP interaction with platelets, PKH26-labeled BDMPs were incubated at 37°C with PRP and an FITC-conjugated antibody against the platelet specific marker CD42b (BD Biosciences) for 30 min and 20 min, respectively. Platelets (CD42b+) were analyzed for PKH26 fluorescence at 567 nm by flow cytometry.

**Electron microscopy:** Purified BDMPs were first fixed in 2.5% of glutaraldehyde for 24 hrs at 4°C, followed by washing with PBS and fixation in 1% of osmium tetroxide for 1.5 hrs at 4°C. They were dehydrated in solutions with increasing concentrations of ethanol and embedded in Epon 812. Ultrathin sections were made and sequentially treated with uranyl acetate and lead citrate before they were dried by heat. The slides were observed under transmission electron microscopy (JEM-1230, Japan). For an enhanced view of the plasma membrane, BDMPs loaded onto carbon-coated formvar grids for 1 min were stained with phosphotungstic acid (pH 6.8) for 2 min. To specifically identify BDMPs, a colloid gold-conjugated goat anti-rabbit antibody was immobilized onto the grids for 20 min. These coated grids were washed and incubated with BDMPs that had been pre-incubated with a rabbit anti-GFAP antibody (ZSGB-Bio, China, 4°C overnight) for 4 hrs before being processed for transmission electron microscopy.

Scanning electron microscopy was also utilized to observe the BDMP-platelet interaction (supplemental method).

**Statistical analysis**
Categorical (frequency) variables were expressed as percentages and continuous variables as the mean ± SEM. Data were analyzed using Sigma plot (V. 11.2) for the paired $t$-test, one way or repeated measures ANOVA as specified in each dataset. A $p$ value of less than 0.05 was considered to be statistically significant.
RESULTS

Development of a BDMP-dependent hyper-coagulable state in TBI mice

At a mean fluid pressure of 1.9 ± 0.1 atm generated from a FPI device, mice sustained cerebral injury visible at the site of impact (Fig. 1A). When measured by a PS-dependent clotting assay, plasma from TBI mice had a significantly shortened (accelerated) clotting time compared to plasma from mice with sham surgery (Fig. 1B). This shortened clotting time was reversed when microparticles were removed from the plasma (Fig. 1C). In parallel with changes in the clotting time, glial cell- (GFAP+) and neuron-derived (NSE+) BDMPs were detected in blood samples from the TBI mice (Fig. 1D & E), but not in mice before being subjected to either FPI or sham surgery (the baseline levels for non-injured mice and IgG isotype controls were at 0.025±0.019% and 0.038±0.016%, respectively). The presence of these BDMPs was further verified by a second set of neuronal (Na+/K+ ATPase α3) and glial cell (glutamate transporter 1) markers (Fig. S5). BDMPs reached peak levels 3 hrs post-injury (Figures 1D & E), with mean levels at 17,496±4,833/μl and 18,388±3,657/μl of GFAP+ and NSE+ microparticles, respectively. The numbers of BDMPs at other time points were calculated by extrapolating values at peak levels 3 hrs post TBI (Fig. S6) and found to be consistent. The level of plasma GFAP+ microparticles decreased 6 hrs post-injury, whereas NSE+ microparticles remained relatively constant. A portion of these BDMPs expressed PS as detected by annexin V (Fig. 1F). The percent of PS+ BDMPs varied considerably among individual mice, accounting for 39 ± 21% and 42 ± 26% of total GFAP+ and NSE+ microparticles, respectively.
BDMPs were also detected in blood samples from mice that had undergone sham surgery (Fig. 1D & E), but reaching peak levels of $1,853 \pm 745/\mu l$ (GFAP$^+$) and $2,153 \pm 889/\mu l$ (NSE$^+$), significantly lower than those found in TBI mice ($n = 12$, $p < 0.01$).

**Procoagulant activity of BDMPs**

Specifically investigating the role of BDMPs in the development of TBI-associated coagulopathy is challenging in mice with FPI, because microparticles from endothelial and blood cells are also released in response to traumatic stress. To overcome this technical challenge, we generated BDMPs from the brains of adult C57BL/6J mice by freeze-thawing injury. The BDMPs thus produced resemble those detected in the plasma of FPI mice in size and levels of PS and GFAP expression (Fig. S7). When viewed under transmission electron microscopy, these BDMPs were irregular spheres of 50-500 nm in diameter, with a clearly defined and relatively intact membrane, but without apparent granules (Fig. 2A). They expressed NSE and GFAP (Fig. 2B) and could be classified as TF$^+$, PS$^+$, and TF$^+$/PS$^+$ microparticles (Fig. 2C). In contrast, we did not detect VWF (Fig. 2B), a common marker for Weibel-Palade bodies of endothelial cells and $\alpha$-granules of platelets that overlap in size (~50-200 nm) and could be co-purified along with BDMPs. The surface markers for leukocytes (CD45), endothelial cells (CD144), and erythrocytes (CD235a) were also negative (Fig. S8), suggesting that the contaminants from blood and endothelial cells were below the detection in these BDMP preparations.
When added to phospholipid-free plasma, BDMPs accelerated the rate of PS-dependent clot formation in a dose-dependent manner, reaching a maximal activity at ~1 x 10^5 BDMPs/μl, which was equivalent to 1.6 μg/μl of purified brain PS (Fig. 2D). This PS-dependent procoagulant activity was blocked by the PS-binding protein lactadherin (Fig. 2E), which bound BDMPs (Fig. S9). The BDMP-lactadherin interaction was partially blocked by purified PS, but not PC (Fig. S10). In comparable numbers, BDMPs were significantly more active in promoting clot formation than the microparticles generated from platelets activated by collagen, which is known to induce platelet microvesiculation (supplemental method, Fig. S11). These platelet microparticles expressed PS, but not TF at a detectable level (Fig. S12). BDMPs also promoted thrombin generation in a TF-dependent assay, where 25,000/μl of BDMPs had an activity equivalent to 1 pM of soluble TF (Fig. 2E). This BDMP-induced thrombin generation had a significantly delayed onset and a smaller AUC (Tab. 1). In both assays, the number of BDMPs that induced a maximal level of coagulation (Fig. 2D & E) was comparable to that detected in FPI mice (Fig. 1D & E).

To specifically measure the procoagulant activity of BDMPs in vivo, we injected BDMPs into uninjured mice through the tail vein and collected blood samples 30 min after injection to measure the rate of clot formation and the level of plasma fibrinogen. The lungs, kidney, and heart were also collected at the same time and evaluated for fibrin deposition, a hallmark of consumptive coagulopathy. In this experimental setting, mice injected with 1 x 10^4/μl of BDMPs showed a tendency toward a shortened clotting time. Further increases in the number of BDMPs resulted in a progressively prolonged
clotting time (Fig. 3A). Consistent with this dose-dependent biphasic hyper-turned hypo-
coagulable state, the plasma level of fibrinogen was progressively reduced by an
increasing number of BDMPs injected (Fig. 3B). Phosphotungstic acide hematoxylin
stain (PTAH) revealed a wide-spread fibrin deposition in the microvasculature of the
lungs, kidney, and heart of the mice injected with BDMPs, but not in the same organs of
mice injected with PBS (Fig. 3C-H). These data show that BDMPs induced a dose-
dependent transition from a hyper-coagulable state to consumptive coagulopathy,
consistent with the phenotype observed in TBI mice and patients with TBI.

**BDMP production by injured brain cells and transmigration through the disrupted
endothelial barrier**

The data have so far shown that injured brain released BDMPs into the systemic
circulation through the traumatized blood-brain barrier (BBB), resulting in intravascular
coagulation. The extravasation of Evans blue was indeed observed in brains dissected
from mice with FPI, but not from those with sham surgery (Fig. 4A). The production and
transmigration of BDMPs were further examined *in vitro*. Cultured hippocampal cells
(Fig. 4B) released microparticles after stimulation with the calcium ionophore A23187
(Fig. 4C), an agent known to induce apoptosis and microvesiculation. The ability of
BDMPs to pass through the endothelial barrier was measured in a transwell system,
where confluent human umbilical cord endothelial cells (HUVECs) cultured in the top
chamber were first activated by histamine (Fig. 4D), which increases vascular
permeability by inducing endothelial cells to contract. BDMPs were then loaded onto
the endothelial cells in the presence or absence of live or lyophilized platelets. After
incubation for 3 hrs at 37°C, the time when the highest level of BDMPs was found in the
blood of FPI mice (Fig. 1), BDMPs were detected in the bottom chamber when they
were incubated with histamine-stimulated HUVECs and live, but not lyophilized platelets
(Fig. 4E). Live platelets also facilitated a lower rate of BDMP transmigration through
unstimulated HUVECs. To further examine a role of platelets in promoting BDMP
transmigration, we tested serotonin, a major component of platelet dense granules that
is released upon platelet activation 47 and is known to enhance the procoagulant
properties of platelets 48 and to increase vascular permeability. 49 As shown in Fig. 4E,
serotonin at 5 μM promoted the transmigration of BDMPs through the endothelial barrier
at a level similar to that induced by live platelets on histamine-stimulated HUVECs.

A role of platelets in assisting the transmigration of BDMPs through activated HUVECs
was further examined by SEM that detected BDMPs on the transwell membrane in the
opposite side of histamine-activated HUVECs incubated with BDMPs with, but not
without platelets (Fig. 4F).

**Effects of BDMPs on platelets**

The data presented in Figure 4E & 4F suggest that platelets assisted the transmigration
of BDMP through a disrupted endothelial barrier. Therefore, we examined if this platelet-
BDMP interaction affected platelet function. BDMPs were detected binding platelets by
flow cytometry (Fig. 5A) and scanning electron microscopy (Fig. 5B). Furthermore,
BDMPs induced rapid and time-dependent calcium influx in platelets that reached a
plateau 15 min after the stimulation (Fig. 5C). Platelets incubated with BDMPs also
expressed CD62p (Fig. 5D) and PS (Fig. 5E). In contrast, BDMPs did not directly induce platelet aggregation or enhance collagen-induced platelet aggregation (Fig. 5F).
DISCUSSION

Acute changes in coagulation associated with TBI were studied using a mouse FPI model combined with reciprocal mouse and complementary in vitro experiments to identify their causes. We focused on the early hours post TBI (≤ 6 hrs) in order to minimize confounding changes induced by secondary events, such as ischemic injury. We made several novel observations that define a causal role for BDMPs in the systemic coagulation associated with TBI in mouse models.

First, mice subjected to FPI developed a hypercoagulable state within 3 hrs of the injury and this hypercoagulable state was reversed when microparticles were removed (Fig. 1). The development of this hypercoagulable state was associated in time with BDMPs reaching peak levels in the circulation. Although widely used as a neuronal marker, NSE is also detected in human serum, platelets and erythrocytes.\textsuperscript{35,36,50} We presented several lines of experimental evidence to the brain origin of these MPs: 1) validation of BDMPs with a second set of neuronal and glial cell markers (Fig. S5) and 90-98% of BDMPs stained positive for both sets of markers; 2) detection of MPs that are positive for GFAP, a much more specific marker for glial cells (Fig. 1E), and 3) identical flow cytometric profiles of BDMPs from TBI mice and those made from mouse brain (Fig. S7). Interestingly, we did not detect NSE in mouse platelet microparticles (Fig. 2B), suggesting that NSE in platelets may not be microparticle-bound.

In reciprocal experiments, uninjured mice injected with BDMPs underwent a rapid and dose-dependent transition from a hyper-coagulable state to a consumptive...
coagulopathy (Fig. 3), as demonstrated by 1) a transition from mildly shortened to significantly prolonged clotting time, 2) a progressive reduction (depletion) of plasma fibrinogen with increasing dosing of BDMPs, and 3) widespread fibrin deposition in the vasculature. The observation that mice subjected to FPI developed a clearly defined hypercoagulable state, whereas coagulopathy rapidly occurred in mice injected with a similar number of BDMPs proceeded with a mild hypercoagulable state (Fig. 1 vs. Fig. 3), suggests that the speed of BDMP release into the circulation is critical for the development of coagulopathy. BDMPs were released over time from a traumatically injured brain, but injected as a bolus (< 5 min) into an uninjured mouse.

The procoagulant activity of BDMPs requires PS and TF on the surface of these microparticles because it was 1) detected in both PS-dependent and TF-dependent coagulation assays (Fig. 2), 2) dose-dependently blocked by the PS-binding protein, lactadherin (Fig. 2), and 3) greater than a comparable number of platelet microparticles that did not have a detectable level of TF (Fig. S4). BDMP-facilitated thrombin generation had a delayed onset and smaller AUC compared to soluble human TF (Fig. 2 & Tab. 1). The distinct kinetics may result from: 1) cooperativity between TF and PS co-expressed on BDMPs, as compared to soluble TF and PS added separately, 2) structural and functional differences between membrane-bound and soluble TF, and/or 3) species differences between BDMP-bound mouse TF and soluble human TF.

Another critical observation is that BDMPs were detected (albeit at a very low level) in mice exposed to sham surgery (Fig. 1), likely due to minor injury associated with the
surgery. The finding suggests that brain cells are highly sensitive to microvesiculation. This residual level of BDMPs had a minimal influence on coagulation in the acute stage of injury (Fig. 1), but its long-term impacts, especially after repeated exposures, remains to be determined.

Second, we have demonstrated that BDMPs activate platelets (Fig. 5). Platelets may facilitate the transmigration of BDMPs through a disrupted endothelial barrier (Fig. 4) by serving as a carrier or by promoting local inflammation at a site of vascular injury. The former is unlikely because the membrane pores used in the culture matrix of the transwell were 0.4 μm in diameter, substantially smaller than activated platelets (5-7 μm) and lyophilized platelets failed to support the transmigration (Fig. 4E). In the latter case, BDMP-activated platelets release pro-inflammatory mediators that can induce or propagate local inflammation. One of such mediators may be seroton as it has been previously reported to increase vascular permeability. This inflammatory activity may explain why live, but not lyophilized platelets, promoted BDMP transmigration through unstimulated endothelial cells. Surprisingly, BDMPs did not directly induce platelet aggregation or enhance its induction by collagen, potentially due to the steric hindrance of BDMPs that prevents platelet-to-platelet contacts.

Third, we demonstrated the ability of lactadherin to block PS-dependent procoagulant activity (Fig. 2E), raising two important perspectives. The first is that PS scavengers and PS-neutralizing molecules, such as lactadherin and annexin V, may reduce TBI-associated coagulopathy and BDMP-induced platelet activation. Annexin V has been
reported to inhibit arterial thrombosis in a rabbit model of carotid artery injury.\textsuperscript{52} The second is that an intrinsic or acquired deficiency in a PS-dependent clearance of microparticles may predispose an individual to TBI-associated consumptive coagulopathy. The molecules involved in the clearance and/or neutralization of PS\textsuperscript{+} microparticles (and apoptotic cells) may thus have predictive and therapeutic values for coagulopathy associated with TBI and other pathologies.

In summary, we show that a traumatically injured brain releases procoagulant BDMPs into the circulation to promote intravascular coagulation and activate platelets. Our results call for clinical studies to detect BDMPs in the systemic circulation of patients with TBI and to investigate their contributions to the development of coagulopathy and clinical outcomes. If validated in clinical studies, BDMPs in the circulation may serve as a predictive marker of TBI-associated coagulopathy and a therapeutic target for its prevention and treatment. Blood cells have been the focus on linking microparticles to the development of coagulation and inflammatory pathologies, but cancer cell-derived microparticles have increasingly been recognized for a role in the development of cancer-associated thrombosis.\textsuperscript{53} Our results further suggest that microparticles from injured tissues/organs contribute to trauma-associated coagulopathy.
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Conflict of interest

The authors claim no conflict of interest related to the study.

Author contributions:

YT: designed and performed experiments, data analysis and manuscript writing
BS: designed and performed experiments, manuscript writing
MW: designed and performed experiments, manuscript writing
HY: designed and performed experiments,
JY: designed and performed experiments
ZZ: designed and performed experiments
XW: designed and performed experiments
YZ: designed and performed experiments, data analysis, manuscript writing
BAK: designed experiments, manuscript writing
PT: generated lactadherin, data analysis, manuscript writing
ML: developed hypotheses, designed experiments, analyzed data, wrote manuscript
JZ: developed hypotheses, designed experiments, analyzed data, wrote manuscript
JFD: developed hypotheses, designed experiments, analyzed data, wrote manuscript
**Tab. 1: Thrombin generation induced by BDMPs**

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<th>Tissue factor (1 pM)</th>
<th>BDMP (2.5 $\times$ 10^4/μl)</th>
<th>p value**</th>
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<tr>
<td>Lag time (min)</td>
<td>4.6 (0.9)</td>
<td>13.0 (2.6)</td>
<td>&lt; 0.001</td>
</tr>
<tr>
<td>Peak conc. (nM)</td>
<td>89.3 (55.9)</td>
<td>90.8 (7.7)</td>
<td>0.23</td>
</tr>
<tr>
<td>AUC (nM/min)</td>
<td>1196.4 (229.2)</td>
<td>300.0 (10.2)</td>
<td>&lt; 0.001</td>
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</table>

*Values are expressed as mean (SD); ** paired t-test
REFERENCE


FIGURES AND LEGENDS

Fig. 1: FPI-induced and BDMP-dependent coagulation: (A) Cerebral injury is visible in the left parietal lobe of a mouse 3 hrs after FPI (1.9 ± 0.1 atm), compared to the brain from a mouse subjected to sham surgery. (B) The clotting time of PPP collected from mice 3 hrs after FPI or sham surgery was measured in a PS-dependent assay (n = 6, paired t-test). (C) Clotting times were compared between PPP and homologous MPFP collected from mice subjected to FPI and sham surgery (n = 9, paired t-test). (D & E) GFAP+ and NSE+ microparticles were detected by flow cytometry over time in blood samples from TBI and sham mice (n = 6 at each time point, and the values are after the subtraction of values from isotype IgGs, one way ANOVA, n = 48, * p < 0.01, ** p < 0.05). (F) Fractions of GFAP+ and NSE+ microparticles that express PS as measured by annexin V binding (a representative of 16 separate experiments).

Fig. 2: Procoagulant activity of BDMPs from freeze-thawing injury: (A) Top: TEM image of BDMPs (bar = 200 nm); insert: a microparticle stained with an immune-gold-labeled GFAP antibody (bar = 100 nm); and bottom: TEM image of BDMPs with negative staining to enhance the view of membrane structures (bar = 200 nm). (B) BDMPs and platelet microparticles solubilized in a SDS lysis buffer were probed for NSE, GFAP and VWF (T: whole brain lysate, Pts: platelet lysate as control). (C) The expression of TF, PS and both was measured for BDMPs (represents 20 separate measurements). (D) PS-dependent clotting time was measured in the presence of increasing numbers of BDMPs (n = 6, one way ANOVA, p < 0.001) and compared to those induced by 1.6 μg/μl of purified brain PS and PC, respectively. (E) Plasma clotting times induced by 25,000/μl BDMPs were measured in the presence of increasing concentrations of bovine lactadherin. (F) TF-dependent thrombin generation was measured in reaction containing either 1 pM TF or 25,000 BDMPs (representative of 3 separate experiments).

Figure 3: Coagulopathy induced by infusion of BDMPs into uninjured mice: (A) Blood samples were collected from mice infused with BDMPs or PBS and tested for PS-dependent clot formation (n = 12, one way ANOVA ** p = 0.036, * p < 0.001 compared
to PBS). (B) Levels of fibrinogen were measured in the plasma samples collected for studies in panel A (n = 12, one way ANOVA, * p < 0.001 compared to PBS). Sections of formaldehyde-fixed lungs, kidney, and heart from mice injected with BDMPs (C - E) or PBS (F - H) were stained with phosphotungstic acid hematoxylin (PTAH, dark blue, the dye also stains muscle cells). The left panel shows fibrin deposition in the microvasculature of the lung (C), kidney (D), and stromatic vessels of the heart (E) from mice injected with BDMPs (arrows). Arrowheads indicate intact walls of fibrin deposited vessels (bar = 25 μm). Fibrin deposition was not detected in organs collected from mice receiving PBS (F - H, bar = 25 μm). Images are representative of 6 mice injected with BDMPs and 5 with PBS.

Fig. 4: Production and transmigration of BDMPs: (A) Evans blue leaked from the vasculature of a mouse subjected to FPI, but significantly less from the one with sham surgery (representatives of 3 pairs of mice). (B) A representative image of hippocampal cells that were cultured for 7 days. (C) Cultured hippocampal cells were stimulated with 50 μM of the calcium ionophore A23187. The media collected before (top left) and after stimulation (top right and bottom left) were analyzed for BDMPs by flow cytometry (n = 6, paired t-test, p < 0.001). (D) HUVECs grown to confluence (left) become retracted and granulated (arrows) after being stimulated with 25 μM histamine (right, bar = 20 μm). (E) PKH26-labeled BDMPs detected in the bottom chamber by flow cytometry 3 hrs after BDMPs were incubated with resting and histamine-activated (His) HUVECs in the presence and absence of 3 x 10^5/μl human live (Pts) or lyophilized (Lyo. Pts) platelets (n = 6/group, one way ANOVA, *p < 0.005 vs. baseline). Serotonin (5 μM) also promotes microparticle transmigration in the absence of live platelets. (F) SEM images showing BDMPs (arrowhead) on the opposite side of the membrane from histamine-activated HUVECs that were incubated with BDMPs in the presence (a) and absence (b) of live platelets or resting HUVECs incubated with BDMPs (c, bar = 5 μm).

Fig. 5: Effect of BDMPs on platelets: (A) Human platelets incubated with PKH26-labeled BDMPs and a CD61 antibody (10 min at 37°C) were gated on CD61 positivity and analyzed for PKH26 fluorescence by flow cytometry (one way ANOVA, n = 12, *p <
0.01 compared to baseline). (B) Scanning electron microscopic images of platelets immobilized onto fibrinogen and incubated with either PBS (left, bar = 1μm) or BDMPs (right, bar = 1μm). (C) Calcium influx in platelets incubated with 25,000/μl BDMPs for the indicated times (n = 6, repeated measures ANOVA, *p < 0.001, the values are after background subtraction). (D) CD62p expression was measured on platelets incubated with 25,000/μl BDMPs for 30 min at 37°C in the presence and absence of type I collagen (n = 6, paired t-test). (E) Annexin V binding to platelets (CD61+) treated with BDMPs was measured by flow cytometry (n = 6, one way ANOVA, *p < 0.001 compared to baseline). (F) Human platelets were monitored for aggregation in an optical aggregometer after 25,000/μl BDMPs were added to 100 μl PRP with and without collagen (n = 6, paired t-test).
Brain-derived microparticles induce systemic coagulation in a murine model of traumatic brain injury

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