Conventional and pretargeted radioimmunotherapy using bismuth-213 to target and treat non-Hodgkin lymphomas expressing CD20: a preclinical model toward optimal consolidation therapy to eradicate minimal residual disease

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Radioimmunotherapy (RIT) with α-emitting radionuclides is an attractive approach for the treatment of minimal residual disease because the short path lengths and high energies of α-particles produce optimal cytotoxicity at small target sites while minimizing damage to surrounding normal tissues. Pretargeted RIT (PRIT) using antibody-streptavidin (Ab-SA) constructs and radiolabeled biotin allows rapid, specific localization of radioactivity at tumor sites, making it an optimal method to target α-emitters with short half-lives, such as bismuth-213 (213Bi). Athymic mice bearing Ramos lymphoma xenografts received anti-CD20 1F5(scFv)SA fusion protein (FP), followed by a dendrimeric clearing agent and [213Bi]DOTA-biotin. After 90 minutes, tumor uptake for 1F5(scFv)SA was 16.5% ± 7.0% injected dose per gram compared with 2.3% ± 9% injected dose per gram for the control FP. Mice treated with anti-CD20 PRIT and 600 µCi [213Bi]DOTA-biotin exhibited marked tumor growth delays compared with controls (mean tumor volume .01 ± .02 vs. 203.38 ± 83.03 mm³ after 19 days, respectively). The median survival for the 1F5(scFv)SA group was 90 days compared with 23 days for the control FP (P < .0001). Treatment was well tolerated, with no treatment-related mortalities. This study demonstrates the favorable biodistribution profile and excellent therapeutic efficacy attainable with 213Bi-labeled anti-CD20 PRIT. (Blood. 2010;116(20):4231-4239)

Introduction

Non-Hodgkin lymphoma (NHL) is the sixth most common type of cancer, with over 74,000 new cases diagnosed annually in the United States.1 Following conventional treatment with chemotherapy or radiation therapy, patients with advanced stage indolent NHL inevitably relapse, with death occurring a median of 5 years after recurrence.2 The introduction of rituximab, a monoclonal antibody against CD20, has led to improved survival in patients with NHL.3-5 Despite the encouraging clinical results with anti-CD20 antibodies, however, the majority of patients with indolent NHL who respond to immunochemotherapy eventually relapse with recurrent lymphoma.5-7 Recently, radioimmunotherapy (RIT) has emerged as a promising treatment option for lymphoma. RIT with iodine-131(131I) tositumomab or yttrium-90 (90Y) ibritumomab tiuxetan as a single agent has yielded excellent overall response rates of 50% - 80%, with complete response rates of 20% - 40% in patients with relapsed or refractory indolent NHL.8-13 Even more notable response rates have been observed when RIT is used as front-line treatment in patients with indolent NHL.14 In a recent large phase 3 trial, the addition of 90Y-ibritumomab tiuxetan in first remission after chemotherapy significantly improved response rates and remission durations in patients with advanced-stage follicular lymphoma,15 presumably by killing residual tumor cells that survived the induction chemotherapy.16 Based on this data, 90Y-ibritumomab tiuxetan has been approved by the FDA for first line consolidation therapy in follicular lymphoma. However, the β-emitting radionuclides used in current RIT schemes may not be ideal for irradiating microscopic tumors and isolated tumor cells present in the setting of minimal residual disease (MRD). It is estimated that the fraction of energy deposited in a tumor measuring 200 µm in diameter is only 1.5% and 17% for 90Y-labeled and 131I-labeled antibodies (Abs), respectively.17,18 The remainder of the β energy is deposited in surrounding normal tissues, resulting in dose-limiting toxicities. Furthermore, the relatively low decay energies of β-particles result in suboptimal killing of tumor cells, ultimately contributing to relapse in the majority of treated patients. In contrast, α-emitting radionuclides impart high-linear-energy-transfer radiation along densely ionized, linear tracks over relatively short distances (40 to 90 µm or few cell diameters), which are highly effective in cell-killing. Alpha-particles are associated with much as 400-fold greater linear energy transfer as β-particles, and cell death may result from transversal of just 1-5 α-particle emissions through the nucleus.19,20 In addition, α-particles induce irreparable double-stranded DNA breaks, which are not amenable to most DNA repair mechanisms present in tumor cells.21 These physical characteristics of α-particles may afford optimal cytotoxicity for small foci of chemoresistant tumor cells while minimizing damage to the surrounding normal tissues in MRD settings.
Our group has successfully demonstrated that pretargeted RIT (PRIT) using antibody-streptavidin (Ab-SA) conjugates and related fusion proteins (FP), followed by radiolabeled biotin provides rapid specific localization of radioactivity at tumor sites.\textsuperscript{22-27} PRIT is particularly attractive for use of short half-lived α-emitting radionuclides, because it allows the delivery of radioactivity to tumor sites before the activity decays. This is important, because 2 of the most promising α-emitting radionuclides in clinical studies, bismuth-213 (\textsuperscript{213}Bi, \textit{t}_{\text{1/2}} = 46.5 minutes) and astatine-211 (\textsuperscript{211}At, \textit{t}_{\text{1/2}} = 7.21 hours), have short half-lives. In this study, we evaluated the biodistributions of \textsuperscript{213}Bi-labeled DOTA-biotin when using a specific (anti-CD20) FP and a non-specific FP in a PRIT protocol. Those results were compared with biodistribution data from \textsuperscript{212}Bi in a conventional RIT protocol, where the Ab was labeled directly. The biodistributions were conducted in mice bearing B-cell NHL (Ramos) xenografts. The efficacy of an orally administered chelator of \textsuperscript{211}Bi (2,3-dimercapto-1-propanesulfonic acid; DMPS) was evaluated as an approach to reduce nonspecific radiation uptake in the kidney. Using the most favorable PRIT schemes defined in the biodistribution experiments, we conducted a preclinical study to evaluate the therapeutic efficacy and toxicity of \textsuperscript{213}Bi in mice bearing small or large tumor burdens.

**Methods**

**Cell lines**

The human Ramos Burkitt lymphoma cell line was obtained from American Type Culture Collection. Cell lines were maintained in log phase growth in RPMI1640 medium supplemented with 10% heat-inactivated fetal calf serum in a 5% CO\textsubscript{2} incubator. Cell viability exceeded 95% by trypan blue exclusion.

**Antibody, fusion proteins, and pretargeting reagents**

The 1F5 (murine anti-CD20) and HB8181 (murine isotype matched nonbinding control) Abs were produced from the respective hybridomas using a hollow fiber bioreactor system in the monoclonal Ab production facility at the Fred Hutchinson Cancer Research Center. The production and purification of 1F5(scFv)-SA fusion protein (FP) has been previously described.\textsuperscript{26} Briefly, 1F5 scFvSA fusion genes were produced by molecularly fusing the single-chain variable regions (scFv) of the murine anti-CD20 1F5 Ab to the full-length genomic SA of Streptomyces avidinii. The SA gene was then joined to the scFv region using a GSGSA peptide linker. The FP was expressed from an IPTG-inducible lac promoter. The resultant FP was then expressed in the periplasmic space of Escherichia coli and spontaneously formed stable soluble tetramers 1F5(scFv)\textsubscript{4}SA with a molecular mass of 174 kDa. The 1F5-SA FP were formulated at a concentration of 2.3 mg/mL in phosphate buffer saline (PBS) containing 5% sorbitol and stored at \textdegree C. CC49(scFv)-SA FP (negative control) was produced by the same method described above. CC49(scFv)-SA recognizes the TAG-72 antigen expressed on most human adenocarcinomas but not on lymphomas.

**Radiolabelling**

As previously described, 1F5 and HB8181 Abs were conjugated with isocyanoato benzyl-CHX-A\textsuperscript{′}.\textsuperscript{26} Briefly, each Ab was demetallated by dialyzing against 50mM HEPES (N-2-hydroxyethylpiperazine-N-2-ethanesulfonic acid) buffer pH 8.5 that had been treated on a Chelex-100 column to remove metals. The Ab was then reacted overnight with 12 equivalents of isothiocyanatobenzyl-CHX-A\textsuperscript{′} (Macrocyclics). The mixture was dialyzed against 150mM saline that had been demetallated by treating with Chelex-100. The final preparation was stored in acid washed vials. The \textsuperscript{212}Bi was obtained from actinium-225 (\textsuperscript{225}Ac, \textit{t}_{\text{1/2}} \sim 10 days) on a MP-50 ion exchange resin from the Department of Energy. The \textsuperscript{213}Bi was eluted into an acid washed vial from the \textsuperscript{225}Ac column with 0.5 mL of fresh, metal free 0.1M HCl (0.1M NaI dissolved in 0.1M HCl). The pH of the eluant was increased by adding 100-250 \textmu L of 500mM metal free Ammonium acetate pH 5.0. For PRIT experiments, 2-10 \textmu L of 3 mg/mL DOTA-biotin was added to the \textsuperscript{212}Bi eluant and reacted for 5 minutes at 80°C. The mixture was then cooled to room temperature and 10 \textmu L of 100mM DTPA was added. After 2 minutes, 100 \textmu L of 1M NaOH was added to neutralize the pH, and the mixture was diluted to injection volume with PBS. An aliquot was removed and checked for binding by an avidin bead assay. For directly labeled Ab, 200-500 \textmu L of 1F5-CHX-A\textsuperscript{−} (3.7 mg/mL) or HB8181-CHX-A\textsuperscript{−} (5.9 mg/mL) was added to the \textsuperscript{212}Bi eluant and allowed to react for 5 minutes at room temperature. This mixture was passed over a PD-10 column that had been equilibrated in PBS. The protein containing fractions were combined and diluted to the final injection volume in PBS. HB8181 was added at 200 \mu g/dose to block non-specific binding. Purity was determined by instant thin-layer chromatography (80% MeOH with 20% 100mM DTPA in water) and/or immunoprecipitation in MeOH/Water (80/20).

**Mouse RIT and PRIT studies**

Female FoxNi\textsuperscript{19} athymic nude mice, aged 6-8 weeks, were obtained from Harlan Sprague-Dawley and housed under protocols approved by the Fred Hutchinson Cancer Research Center Institutional Animal Care and Use Committee. For all pretargeting experiments, animals were placed on a biotin-deficient diet (Purina Mills) 4-5 days before treatment and maintained on the diet up to 7 days following radiobiotin administration.

**Biodistribution studies**

Ramos cells (10 \times 10\textsuperscript{6}) were injected subcutaneously in the right flank 7 days before FP injection to obtain lymphoma xenografts. Groups of 5 mice with similar, palpable tumors were chosen and were injected intravenously with 2.8 nmol of either 1F5(scFv)-SA or the negative control CC49(scFv)-SA FP. After 20 hours, 50 \mu g of a biotinylated N-acetyl-galactosamine clearing agent (NAGB CA)\textsuperscript{22} was administered intravenously followed 4 hours later by 1.2 mmol (1 \mu g) DOTA-biotin labeled with 20 \mu Ci (0.74 MBq) of \textsuperscript{212}Bi. Blood samples, tumors, and normal organs were obtained and counted for \textsuperscript{212}Bi activity as described previously.\textsuperscript{22}

**Renal uptake studies**

Groups of 5 mice received DMPS (Sigma-Aldrich) in the drinking water (1.2 mg/mL) 24 hours before \textsuperscript{212}Bi-DOTA-biotin. The control animals received regular drinking water. The biodistribution experiments were performed as described above.

**Dosimetry**

All biologic retention data in percentage of injected dose per gram (% ID/g) for each organ or tissue were “un-decay corrected” to effective retention by applying the physical decay constant for \textsuperscript{212}Bi. The time-sequential data for each organ or tissue were then plotted graphically. The data were fitted to biexponential functions of the form \( y = a \exp(-b \times x) + c \exp(-d \times x) \) by linear least-squares regression analysis, with all data points weighted equally. Each best-fit biexponential function was then integrated analytically from time zero to infinity to calculate the area-under-curve, equivalent to the total decays taking place in the organ or tissue per unit administered activity (\mu Ci-hours per \mu Ci). The area-under-curve values were then multiplied by the mean energy emitted per decay for \textsuperscript{212}Bi (19.44 g-CGy/\mu Ci). This equilibrium dose constant includes all alpha and electron particle emissions were assumed to be absorbed locally in the tissue of origin. The product of this multiplication is the radiation absorbed dose per unit administered activity, in units of g-CGy per \mu Ci \textsuperscript{212}Bi administered to the mouse.

**Therapy studies**

The therapeutic efficacy of \textsuperscript{212}Bi using the pretargeted approach was evaluated in groups of 5-10 mice. CC49(scFv)-SA FP was used as a...
negative control. Ramos cells (10 x 10^6) were injected subcutaneously in the right flank 7 days before FP injection to obtain lymphoma xenografts measuring 6-10 mm in diameter. Mice were injected intraperitoneally with anti-asialo GM1 antiserum (30 μL; WAKO) 8 days and 1 day before FP injection to minimize natural killer cell activity in athymic mice and prevent spontaneous tumor regression. Mice with similar, palpable tumors were chosen and randomized for the studies. Mice received DMPS in the drinking water (1.2 mg/mL) 24 hours before [213Bi]DOTA-biotin and continued for another 24 hours after [213Bi] injection. Mice were given 2.8 nmol of either 1F5(scFv)SA or the negative control CC49(scFv)SA FPs followed by 5.8 nmol (50 μg) CA 20 hours later. A single dose of 1.2 nmol (1 μg) DOTA-biotin labeled with 200, 600, or 800 μCi (7.4, 22.2, and 29.6 MBq, respectively) [213Bi]DOTA-biotin was administered 4 hours later. In a second set of experiments, mice were injected with 5 x 10^6 of Ramos cells in the right flank. Mice with similar, visible tumors (≥ 4 mm) were chosen for the studies and randomized into various treatment groups of 5 to 10 mice. After 3 days, mice received DMPS in the drinking water (1.2 mg/mL) and 2.8 nmol of either 1F5(scFv)SA or the negative control CC49(scFv)SA FP. Twenty hours later, 5.8 nmol (50 μg) CA was administered to each animal, followed 4 hours later by 1.2 nmol (1 μg) DOTA-biotin labeled with either 200 μCi or 600 μCi 213Bi (7.4 and 22.2 MBq, respectively). Injections were given intravenously in all therapy studies. Mice were assessed every other day for tumor volume measurements, weight change, and general appearance. Mice were euthanized if xenografts exceeded 10% of total body weight, caused obvious discomfort, or impaired ambulation.

Toxicity studies
Weight loss was used as a measure of general well being. Mice were analyzed for “huddling” behavior, diarrhea, lethargy, and other signs of debility. Toxicity assessments measuring leukocyte count, hemoglobin, and platelet counts, plus aspartate aminotransferase (AST), alanine aminotransferase (ALT), creatinine, and blood urea nitrogen (BUN) levels, were performed on days 14, 28, and 120 from the 213Bi-labeled reagent injection, plus aspartate aminotransferase (AST), alanine aminotransferase (ALT), creatinine, and blood urea nitrogen (BUN) levels. Mice were euthanized if xeno-

Biodistributions
The biodistribution of [213Bi]DOTA-biotin after pretargeting with 1F5(scFv)SA FP was evaluated in athymic mice bearing B-cell NHL xenografts. Groups of 5 mice were administered 2.8 nmol of either 1F5(scFv)SA or CC49(scFv)SA (negative control) FP intravenously. Twenty hours later, mice received 5.8 nmol (50 μg) of CA, followed 4 hours later by 1.2 nmol of [213Bi]DOTA-biotin. At 10, 45, 90, or 180 minutes after injection of [213Bi]DOTA-biotin, mice were killed, and tissues were harvested and counted in a gamma counter to determine the percentage of injected dose per

Figure 1. Biodistribution of [213Bi]DOTA-biotin in tumor, blood, and normal organs after PRT with 1F5-SA or CC49-SA FPs. Athymic mice bearing Ramos xenografts were injected with 2.8 nmol each unlabeled FP followed 20 hours later by 5.8 nmol CA, and 4 hours after that by 1.2 nmol [213Bi]DOTA-biotin. Groups of 5 mice were euthanized 10, 45, 90, and 180 minutes after the injection of [213Bi]DOTA-biotin. The radioactivity in the tissues were quantified by gamma counting, corrected for decay, and expressed as the % ID/g of tissue.

Figure 2. Biodistribution of radioactivity in tumor, blood, and normal organs of athymic mice bearing Ramos xenografts injected with either 1F5 or HB8181 Abs directly labeled with [213Bi]. Groups of 5 mice were injected with 1.4 nmol either conventional trace-labeled 1F5 or HB8181 Abs. Mice were euthanized 10, 45, 90, and 180 minutes after injection of each [213Bi]-labeled Abs. The radioactivity in tumor, blood, and normal organs were quantified by gamma counting, corrected for decay, and expressed as the % ID/g of tissue.

The biodistribution of [213Bi]DOTA-biotin after pretargeting with 1F5(scFv)SA FP was evaluated in athymic mice bearing B-cell NHL xenografts. Groups of 5 mice were administered 2.8 nmol of either 1F5(scFv)SA or CC49(scFv)SA (negative control) FP intravenously. Twenty hours later, mice received 5.8 nmol (50 μg) of CA, followed 4 hours later by 1.2 nmol of [213Bi]DOTA-biotin. At 10, 45, 90, or 180 minutes after injection of [213Bi]DOTA-biotin, mice were killed, and tissues were harvested and counted in a gamma counter to determine the percentage of injected dose per
control. Maximum tumor uptake for 1F5 Ab was 3.0% ± 0.9% ID/g after 180 minutes versus 2.3% ± 0.7% ID/g for the control Ab (P = .171). The blood concentration of [213Bi]1F5-Ab was 37.7% ± 5.0% ID/g after 10 minutes and remained elevated up to 180 minutes after injection (23.2% ± 3.0% ID/g), indicating that the majority of radioactivity was retained in blood during this period. Because of high activity in blood, the content of 213Bi was significantly lower levels of radioactivity in the kidneys compared with the untreated controls at all time points (Figure 4). The renal uptake of 213Bi was 2.3 ± 0.3 for mice treated with DMPS, compared with 6.1 ± 0.8 for mice in the standard PRIT group after 45 minutes. The tumor uptake in DMPS-treated mice appeared to be slightly lower than in untreated mice (P = .025), but the tumor-to-kidney ratios were more favorable for the DMPS-treated group (P = .008). The radiation-absorbed dose per unit of administered activity was calculated based on the biodistribution data using the Medical Internal Radiation Dose method (Figure 5). In DMPS-treated mice, the total absorbed dose was estimated to be

Renal uptake and dosimetry

The efficacy of chelation of 213Bi with DMPS administered in the drinking water was evaluated to reduce nonspecific uptake in the kidney. Earlier studies have shown that DMPS, a metal chelator, is effective in clearing the radioactive alpha daughters of 225Ac, including 213Bi.29 In this study, mice were treated with DMPS orally 24 hours before [213Bi]DOTA-biotin injection, and the biodistribution was evaluated. DMPS-treated mice displayed significantly lower levels of radioactivity in the kidneys compared with the untreated controls at all time points (Figure 4). The renal uptake of 213Bi was 2.3 ± 0.3 for mice treated with DMPS, compared with 6.1 ± 0.8 for mice in the standard PRIT group after 45 minutes. The tumor uptake in DMPS-treated mice appeared to be slightly lower than in untreated mice (P = .025), but the tumor-to-kidney ratios were more favorable for the DMPS-treated group (P = .008). The radiation-absorbed dose per unit of administered activity was calculated based on the biodistribution data using the Medical Internal Radiation Dose method (Figure 5). In DMPS-treated mice, the total absorbed dose was estimated to be

Table 1. Tumor-to-normal organ ratios using conventional RIT or PRIT with Bismuth-213 at 10, 45, 90, and 180 minutes

<table>
<thead>
<tr>
<th>Organ</th>
<th>10 min (RIT)</th>
<th>PRIT</th>
<th>10 min (PRIT)</th>
<th>180 min (RIT)</th>
<th>PRIT</th>
</tr>
</thead>
<tbody>
<tr>
<td>Blood</td>
<td>0.03 ± 0.01</td>
<td>0.06 ± 0.01</td>
<td>16.50 ± 7.73</td>
<td>0.09 ± 0.03</td>
<td>38.31 ± 18.55</td>
</tr>
<tr>
<td>Lung</td>
<td>0.11 ± 0.05</td>
<td>2.41 ± 0.24</td>
<td>0.17 ± 0.04</td>
<td>15.25 ± 6.90</td>
<td>0.24 ± 0.08</td>
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<tr>
<td>Liver</td>
<td>0.08 ± 0.05</td>
<td>5.20 ± 0.46</td>
<td>0.15 ± 0.10</td>
<td>18.23 ± 7.65</td>
<td>0.21 ± 0.12</td>
</tr>
<tr>
<td>Spleen</td>
<td>0.13 ± 0.02</td>
<td>6.52 ± 0.39</td>
<td>0.2 ± 0.07</td>
<td>13.93 ± 6.08</td>
<td>0.28 ± 0.09</td>
</tr>
<tr>
<td>Stomach</td>
<td>0.8 ± 0.10</td>
<td>8.63 ± 5.22</td>
<td>1.9 ± 0.47</td>
<td>53.49 ± 33.74</td>
<td>2.38 ± 1.08</td>
</tr>
<tr>
<td>Kidney</td>
<td>0.11 ± 0.02</td>
<td>0.79 ± 0.04</td>
<td>0.13 ± 0.02</td>
<td>1.68 ± 0.81</td>
<td>0.14 ± 0.05</td>
</tr>
<tr>
<td>Small intestine</td>
<td>0.87 ± 0.24</td>
<td>6.49 ± 1.24</td>
<td>0.97 ± 0.21</td>
<td>18.57 ± 9.93</td>
<td>1.08 ± 0.47</td>
</tr>
<tr>
<td>Colon</td>
<td>2.11 ± 0.68</td>
<td>9.11 ± 0.77</td>
<td>3.29 ± 1.42</td>
<td>70.84 ± 24.40</td>
<td>2.47 ± 1.23</td>
</tr>
</tbody>
</table>

Tumor-to-normal organ ratios using conventional RIT with 213Bi-labeled 1F5 Ab or PRIT with 213Bi-DOTA-biotin following 1F5-SA FP. Groups of 5 mice were used to generate mean values. Data were normalized for tissue weight and corrected for radioactive decay.
Two RIT studies were performed to evaluate the therapeutic efficacy of $^{213}\text{Bi}$ using 2 different xenograft models with low and high tumor burdens. In the first therapy study, female athymic mice were injected subcutaneously with Ramos cells ($10 \times 10^6$) resulting in development of large palpable tumors (~6-10 mm in diameter) 7 days after tumor cell inoculation. Mice were randomized into 5 different groups, all of which received oral DMPS 24 hours before treatment with $^{213}\text{Bi}$. Animals were then injected with either 1F5(scFv)$_4$SA FP or the negative control CC49(scFv)$_4$SA FP followed by NAGB clearing agent. Treatment groups of 5 to 10 mice each received a single injection of 200, 600, or 800 $\mu$Ci $^{213}\text{Bi}$DOTA-biotin 4 hours after the administration of clearing agent. The CC49 negative control group was only tested at the highest dose (800 $\mu$Ci).

The mean tumor sizes were not statistically significantly different between the groups at the initiation of the experiment ($P > .2$). As expected, the untreated control mice showed exponential growth of the lymphoma xenograft, requiring euthanasia in all mice by day 20 (Figure 6). Mice treated with 1F5(scFv)$_4$SA FP followed by $^{213}\text{Bi}$DOTA-biotin exhibited dose-dependent tumor responses. Tumor volumes 19 days after $^{213}\text{Bi}$ treatment were 35.0 ± 20.9 mm$^3$, 26.2 ± 24.8 mm$^3$, and 11.6 ± 12.6 mm$^3$ for 200, 600, and 800 $\mu$Ci of $^{213}\text{Bi}$ treatment groups, respectively, which were significantly smaller than the untreated group (237.9 ± 58.5 mm$^3$). In comparison, mice treated with nonbinding control CC49(scFv)$_4$SA FP followed by $^{213}\text{Bi}$DOTA-biotin showed tumor growth patterns similar to the untreated mice, confirming the specificity of PRIT efficacy. All mice treated with the negative control CC49(scFv)$_4$SA FP and 800 $\mu$Ci $^{213}\text{Bi}$DOTA-biotin were euthanized by day 20 due to uncontrolled tumor growth. Mice treated with 1F5(scFv)$_4$SA FP followed by 200 or 400 $\mu$Ci $^{213}\text{Bi}$DOTA-biotin experienced longer survivals than the control groups ($P < .05$), though tumors rapidly recurred, leading to euthanasia by day 45 in all mice. Three of the 10 mice treated with 1F5(scFv)$_4$SA FP and 800 $\mu$Ci $^{213}\text{Bi}$DOTA-biotin achieved complete regression of tumors by day 20, and one mouse experienced prolonged progression-free survival without tumor recurrence for the duration of the experiment (>120 days). There was no evidence of significant toxicity or weight loss in mice treated with 200 or 600 $^{213}\text{Bi}$DOTA-biotin; however, one mouse treated with 800 $\mu$Ci $^{213}\text{Bi}$DOTA-biotin showed signs of early toxicity with a loss of approximately 10% of its body weight (Figure 6C).

The second therapy study was designed to more closely mimic a MRD setting by using a xenograft model with smaller tumor burdens. Athymic mice were injected with $5 \times 10^6$ Ramos cells in the flank. Three days after cell inoculation, tumors were present and animals with similar-sized, small tumors (~4 mm in diameter)
were randomized into 5 groups. Mice were treated with oral DMPS and FP followed 20 hours later by NAGB CA as described above. A single dose of 200 or 600 µCi \(^{213}\text{Bi}\)DOTA-biotin was injected 4 hours after the CA in groups of 5 to 10 mice. Mice received no higher than 600 µCi of \(^{213}\text{Bi}\) due to possible early toxicities with weight loss observed at 800 µCi dose in the earlier experiment described above.

Control mice receiving either no treatment or treatment with the non-binding CC49(scFv)\(_\text{SA}\) FP followed by \(^{213}\text{Bi}\)DOTA-biotin exhibited exponential growth of tumors as before, necessitating euthanasia by day 25 in all mice (Figure 7). Mice receiving CC49(scFv)\(_\text{SA}\) FP and 600 µCi of Bi-213-labeled DOTA biotin exhibited a modest delay in tumor growth (95.5 ± 39.4 mm\(^3\) after 16 days) compared with the untreated mice (275.8 ± 67.6 mm\(^3\); \(P = .0018\)). Mice treated with 1F5(scFv)\(_\text{SA}\) FP followed by 200 or 600 µCi \(^{213}\text{Bi}\)DOTA-biotin exhibited significant delays in tumor growth (1.1 ± 2.5 mm\(^3\) and 9.2 ± 9.5 mm\(^3\), respectively, at day 16) compared with the control groups (\(P < .01\)). Complete tumor regressions were achieved in 8 of 10 animals receiving 1F5(scFv)\(_\text{SA}\) FP and 600 µCi \(^{213}\text{Bi}\)DOTA-biotin and in 6 of 10 mice treated with 200 µCi \(^{213}\text{Bi}\)DOTA-biotin. The median survival for the group receiving 1F5(scFv)\(_\text{SA}\) FP and 600 µCi \(^{213}\text{Bi}\)DOTA-biotin was 90 days compared with median survivals of 19 days (\(P < .0001\)) and 23 days (\(P < .0001\)) for untreated mice and mice treated with CC49(scFv)\(_\text{SA}\) FP and 600 µCi \(^{213}\text{Bi}\)DOTA-biotin, respectively. The treatment was well tolerated, with no treatment-related mortalities in any group. Leukocyte counts, hemoglobin, and platelet counts in mice receiving 1F5(scFv)\(_\text{SA}\) FP and 600 µCi \(^{213}\text{Bi}\)DOTA-biotin were similar to those of the age matched controls on days 14, 28, and 120 of treatment (Table 2). Transaminase levels appeared slightly higher in the treated mice (\(P < .01\)), but there were no significant differences in creatinine or BUN (data not shown) detected between the treated and the age-matched control mice at days 14, 28, and 120 after the \(^{213}\text{Bi}\) injection. All laboratory values remained stable in the treated mice until the end of observation in this study (> 120 days), suggesting the absence of significant hematologic, hepatic, or renal toxicities during the period of observation.

### Discussion

In this study, we assessed the biodistribution, therapeutic efficacy, and toxicity profile of the \(\alpha\)-emitting radionuclide \(^{213}\text{Bi}\) targeted to the CD20 antigen in a mouse lymphoma xenograft model. Our study showed that conventional RIT with directly labeled \(^{213}\text{Bi}\)F5-Ab was not effective in delivering \(^{213}\text{Bi}\) to the tumor due to the protracted circulating half-life of radiolabeled Ab, making \(^{213}\text{Bi}\) less suitable for conventional RIT because of the short half-life of the radionuclide. These results were concordant with our previous experiments using other radionuclides, which showed maximal targeting of radiolabeled intact Ab to tumor xenografts requires 20 to 24 hours. In marked contrast, the pretargeted approach delivered high levels of radiation rapidly to tumor sites while minimizing nonspecific radiation exposure to normal organs. Furthermore, our study demonstrated that anti-CD20 PRIT using \(^{213}\text{Bi}\) could effectively kill lymphoma cells with regression of tumors and significant prolongation of survivals in all treated mice. As expected, the \(\alpha\)-emitting radionuclide \(^{213}\text{Bi}\) was more effective for small tumors with approximately 40% of mice achieving long term remissions with 600 µCi of \(^{213}\text{Bi}\) compared with no long term remissions in mice with larger tumor volumes treated at this dose. Systemic therapy with \(\leq 600\) µCi \(^{213}\text{Bi}\) was well tolerated with minimal toxicities during the period of observation, as indicated by serial weight and blood test monitoring on days 14, 28, and 120 after treatment.

Recently, increasing data have accrued supporting the importance of eliminating small residual numbers of lymphoma cells following induction chemotherapy in order to achieve long-term disease remissions.\(^{30-32}\) Even after achieving a complete clinical and radiologic remission, microscopic foci of tumor cells may escape the cytotoxic effects of chemotherapy and result in MRD leading to recurrent disease and the eventual emergence of drug-resistant tumors. High-dose myeloablative chemotherapy...
regimens given with stem cell support significantly reduces the risk of relapse by potentially eliminating MRD, but this approach is associated with significant treatment-related mortality and morbidity.¹¹ Immunotherapy with the anti-CD20 Ab, rituximab, has been evaluated as consolidation or maintenance therapy after first-line chemotherapy with some promising results³⁴-³⁶; however, resistance to rituximab is common and the safety of long-term rituximab therapy remains unknown. The exquisite sensitivity of lymphoma cells to radiation makes RIT an especially promising option for consolidation after chemotherapy to eradicate small numbers of chemotherapy-resistant tumor cells, as indicated by results of a recent multicenter randomized trial.¹⁵,¹⁶

Although encouraging results have been obtained with conventional RIT using β-emitting radionuclides such as ¹³¹I and ⁹⁰Y, it is conceivable that alternative radionuclides will prove superior for clinical situations in which multiple micrometastases or isolated tumor cells are present. Alpha-emitting radionuclides with high-linear energy transfer and short path lengths have many theoretical advantages in the setting of MRD³⁷-⁴¹ and have produced exciting results in intraperitoneal and xenograft tumor models and patients with AML, ovarian cancer, and gliomas.⁴²-⁴⁷ Supiot et al.⁴⁸ conducted a study comparing the efficacy of the B-B4 (anti-syndecan-1) Ab labeled with either ²¹³Bi or ¹³¹I for therapy of multiple myeloma. RIT with ²¹³Bi-B-B4 demonstrated cell killing that was dose-dependent, whereas ¹³¹I-labeled B-B4 exhibited minimal cytotoxicity. Behr et al evaluated CO17-1A Fab’ fragments labeled with either ²¹³Bi or ⁹⁰Y in a metastatic GW39 human colon cancer xenograft model in athymic mice.⁴⁹ At maximally tolerated doses, cure rates were 95% for ²¹³Bi and 20% for ⁹⁰Y. The results are consistent with the results reported by Bloomer et al, demonstrating better therapeutic results with an α-emitting (²¹¹At) radionuclide than with β-emitting radionuclides for therapy of malignant ascites.⁵⁰ Taken together, these results demonstrate that α-emitting radionuclides may be superior to β-emitting radionuclides for treatment of microscopic disseminated diseases.

Due to availability and decay properties, only a few α-emitting radionuclides are considered suitable for in vivo applications. The α-emitting radionuclides, ²¹¹At (t₁/₂ = 7.2 hours), ²¹²Bi (t₁/₂ = 60.6 minutes) and ²¹⁳Bi (t₁/₂ = 45.6 minutes) have been considered most favorable³⁷,⁴⁰ because they do not produce daughter radionuclides that also decay by α-emission. However, the very short half-lives and limited availability of those radionuclides may pose challenges in clinical settings. Despite these hurdles, several investigators have successfully conducted clinical trials with α-emitters. Juric and Scheinberg have treated 18 acute myeloid leukemia (AML) patients in a phase 1 trial with a ²¹³Bi-labeled humanized anti-CD33 Ab (HuM195) demonstrating reduction in bone marrow leukemic burden in 14 of 18 evaluable patients. Myelosuppression and transaminitis were routinely observed, but reversible.⁴¹ In a subsequent study, 20 AML patients were safely treated with ²¹³Bi-HuM195 following cytarabine with significant reductions in leukemic blast levels after the delivery of the radiolabeled Ab in the majority of patients.²¹ Despite these encouraging pilot trials, several investigators have concluded that the optimal application of short-lived α-emitters will require novel methods of isolate delivery such as PRIT.²¹,⁴⁰ Initial investigations exploring the utility of pretargeting for ²¹³Bi used an anti-CD25 scFv-SA FP and ²¹³Bi-labeled DOTA-biotin.⁵¹,⁵² This study demonstrated the curative potential of this approach for mice with acute T-cell leukemia and the superiority of ²¹³Bi compared with ⁹⁰Y in a disseminated leukemia model. Other investigators have reported tumor growth inhibition and prolongation of survival in mice bearing A431 epidermoid carcinomas that were treated with anti-Ley B3 Ab-SA conjugates followed by ²¹³Bi-labeled DOTA-biotin.⁵³ Our study demonstrates that systemic therapy with ²¹³Bi using the PRIT approach can lead to prolonged complete remissions of lymphoma xenografts with minimal toxicities in a preclinical model.

Toxicity and pharmacokinetic studies with ²²⁵Ac-Hu195 in mice and cynomolgous monkeys and with pretargeted α-emitters including ²¹³Bi and ²¹³Po⁵³,⁵⁴ suggest that renal tubular damage may be the principal toxicity of this approach.²⁹,⁵⁵ Therefore, we evaluated the efficacy of DMPS to reduce nonspecific uptake of ²¹³Bi in the kidney by providing it in the drinking water. Jaggi et al reported that DMPS could reduce approximately 60% of ²¹³Bi accumulation in the kidney after intravenous injection of an ²²⁵Ac “nano-generator.”²⁹ The current study demonstrates similar efficacy of DMPS with approximately 60% reduction of the total absorbed radiation dose in the kidneys. A recent study by Bäck et al reported that a mean absorbed dose to the kidney of approximately 10 Gy seemed to be acceptable, corresponding to approximately 50% reduction in GFR, in RIT using α-emitting radionuclides.⁵⁶ In our study where DMPS was administered in the drinking water, the absorbed dose to the kidneys per unit administered activity was 0.7 cGy/µCi (4.2 Gy at 600 µCi ²¹³Bi), which delivered substantially less radiation than the reported tolerable α-particle dose of 10 Gy. The lack of significant nephrotoxicity documented here by evaluating serum BUN and creatinine is encouraging. Last, the generally shorter half-lives, shorter range, and higher linear energy transfer of α-emitters could complicate the measurement of dosimetry.²¹ Conventional Medical Internal Radiation Dose methods that estimate mean absorbed dose over a specific organ volume may not always yield biologically meaningful information because the high energy of α particles delivered over a short range may result in targeted cells receiving high doses whereas neighboring cells may receive no radiation exposure. Therefore, we are currently evaluating a novel method using α-particle imaging to...
better determine the small-scale dosimetry of α-emitting radionuclides.37

In summary, the current study demonstrates that systemic therapy with α-emitting radionuclides using a pretargeted approach is feasible and effective for treatment of non-Hodgkin lymphoma. The results appear promising with significant tumor regressions and prolonged survivals especially in mice bearing relatively small albeit macroscopic tumors. We anticipate that this treatment method would be even more effective in eliminating microscopic foci of residual lymphoma cells and micrometastases. We are currently evaluating studies using α-PRIT directly compared with β-PRIT following initial chemotherapy in a true MRD setting.

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Authorship

Contribution: S.I.P. designed and performed research, analyzed data, and wrote the paper; J.S. performed research and analyzed data; J.M.P. and D.S.W. interpreted research and analyzed and interpreted data; D.K.H. contributed vital reagents and performed research; N.O., A.L.K., S.F., and A.A. performed research and collected data; T.B. conceived and designed research; Y.L. contributed vital reagents; D.R.F., A.K.G. and D.J.G. interpreted data; and O.W.P. conceived and designed research, analyzed and interpreted data, and revised the paper.

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Conventional and pretargeted radioimmunotherapy using bismuth-213 to target and treat non-Hodgkin lymphomas expressing CD20: a preclinical model toward optimal consolidation therapy to eradicate minimal residual disease